

## 2.1 Instrumentation

# Magnetism & MR Magnets

& other MR system components: shim systems, RF system, gradient system, other components

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## Outline

- Magnetism
- MR Magnets
  - Permanent
  - Resistive
  - Super-conducting
- Shim System
- Gradient System
- RF System

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Slide # 2

## Objectives

Upon completion of this course, the attendee should...

1. Have an understanding of magnetism & magnetic properties
2. Understand various MR imagers
3. Have an understanding various system components
4. Learn the difference between magnet, shim, gradients and RF systems
5. Understand various MR components, their "job" and operation.

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Slide # 3

## Magnetic System Components

- The Main Magnet (Bo)
- The Shim Magnet
- The Gradient Magnet
- The RF Magnet (B1)
- And you thought that there was only one!



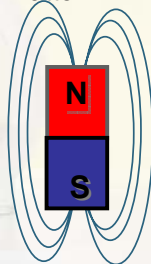
Image courtesy of Philips Medical

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## Magnetism

- Fundamental property of matter
  - Like mass
  - Like charge
- Magnetic Susceptibility
- Magnetic Properties



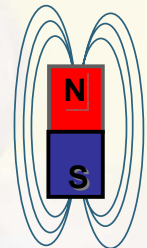
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## Magnetic susceptibility

The ability for a material to become magnetized

- Diamagnetic materials
- Paramagnetic materials
- Super paramagnetic materials
- Ferromagnetic materials



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### Diamagnetic Materials

**Dia-Magnetic Characteristics**

- Paired Electrons
- Electron Cloud protects nucleus
- Negative susceptibility
- Low susceptibility
- "D"oes not fly into the magnet

**Dia-Magnetic Material**

- Wood
- Glass
- Plastic
- Metals
- gold
- silver
- Stainless Steel

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### Paramagnetic Materials

**Para-Magnetic Characteristics**

- Unpaired Electrons
- no protection for the nucleus
- Positive susceptibility
- Low susceptibility

**Para-Magnetic Material**

- Gadolinium contrast agents

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### Ferromagnetic Materials

**Ferro-Magnetic Characteristics**

- $\frac{1}{2}$  filled Electron shells
- no protection for the nucleus
- Positive susceptibility
- High susceptibility
- "F"lies into the magnet

**Ferro-Magnetic Material**

- Iron
- Steel

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### Magnetic Properties

**Dia-Magnetic**

- Wood
- Plastic
- Glass

**Para-Magnetic**

- gadolinium
- manganese

**Super Paramagnetic**

- Contrast agents
- Iron Oxide
- T2 agents

**Ferro-Magnetic**

- Iron
- Steel

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### How to Make a Magnet

**Permanent magnets**

Magnetize ferromagnetic materials  
Permanently magnetized

**Electromagnets**

Current in wires  
Requires current to remain magnetized

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### Right Hand Thumb Rule

**B = magnetic field**

**e = electrons flowing in current**

**I = current**

- Wrap fingers of right had around the wire
- Point thumb in the direction of current
- Fingers point in the direction of the magnetic field (B)

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### Solenoid Electromagnet

Strength of the magnetic field of a solenoid  
 $\frac{2 \pi N I}{\text{space}} = B$

$I$  = current  
 $B$  = magnetic field

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### Magnetic Field Strength

- Tesla (T)
  - Within the bore
- Gauss (g)
  - Outside the imager
- 1T = 10,000 g

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### "Magnetic"

- The Main Magnet ( $B_0$ )
  - Static magnetic field
  - Magnetize the proton spins
- The Shim Magnet
- The Gradient Magnet
- The RF Magnet ( $B_1$ )

Image courtesy of Philips Medical

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### Magnet Configurations

Image courtesy of Hitachi Medical  
Permanent Magnet 0.3T

Image courtesy of Philips Medical  
Resistive Magnet 0.3T

Image courtesy of Siemens Medical  
Superconducting Magnet 1.5T

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### Simple Permanent Magnet Configurations

- Horseshoe Magnets
- Face – to- face
- Vertical field
- "Open"

Image courtesy of Hitachi Medical

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### Permanent Magnet

Vertical Field

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### Permanent Magnet Imager

- Magnetic material magnetized
- Permanently magnetized
  - Always on
- Temperature sensitive
- Heavy in weight
- Low field strength
- Vertical field

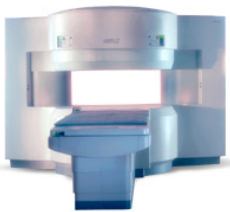



Image courtesy of Hitachi Medical

Permanent Magnet 0.3T

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### Permanent Magnet Imagers



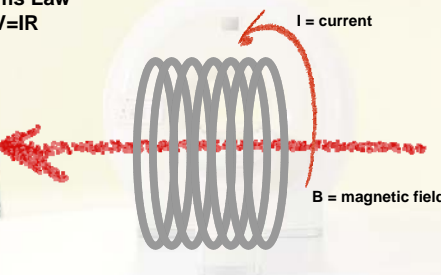
Hitachi Airis (0.3 T)      GE Profile (0.2 T)

Images courtesy of Hitachi and GE Medical Systems

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### Resistive Magnet

**Ohms Law**  
 $V=IR$

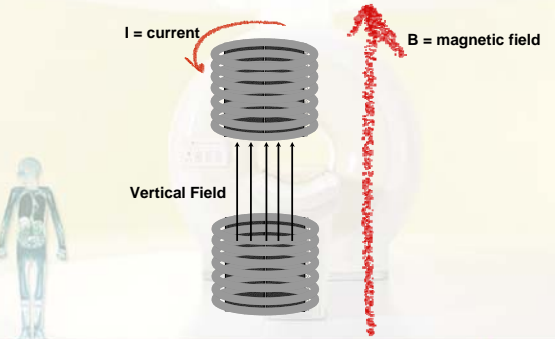


$I = \text{current}$

$B = \text{magnetic field}$

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### Iron Core Resistive Magnet



$I = \text{current}$

$B = \text{magnetic field}$

Vertical Field

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### Resistive Magnet Imager

- Electro-Magnet
  - Current within conductors
  - Resistance within the conductors
- Requires current to be on
  - Can be turned off
- Light in weight
- Low field strength
- Vertical or Horizontal field





Image courtesy of Philips Medical

Resistive Magnet 0.3T

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### Upright System



Transverse field

Image courtesy of Fonar

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### Superconducting Magnet

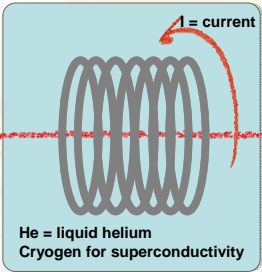


Image courtesy of Siemens Medical

Clinical Imagers with field strengths up to 3.0 T  
Research systems at 7.0 T and >


He = liquid helium  
Cryogen for superconductivity

$I$  = current  
 $B$  = magnetic field

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### Superconducting Magnet Imager

- Superconducting Electro-Magnet
  - Current within conductors
  - Supercooled to remove resistance
  - Needs cryogenics (liquid helium)
- Always on
- High field strength
- Horizontal field
  - Rare exceptions




Helium Turrent & bursting disk

Image courtesy of Philips Medical

Superconducting Magnet 1.5T

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### High Field Extremity Magnet



Images courtesy of ONI Medical Systems

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### Whole Body Superconducting Hybrid Magnet



Images courtesy of GE

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### Magnetic Field Shielding

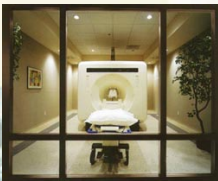


Image courtesy Lindgren

- Passive
  - Metal in scan room walls
- Active
  - Implies current
  - Other magnets within
- 5 g within the wall

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### Magnetic System Components

- The Main Magnet ( $B_0$ )
- The Shim Magnet
- The Gradient Magnet
- The RF Magnet ( $B_1$ )




Image courtesy of Philips Medical

- And you thought that there was only one magnet in the MR Imager!

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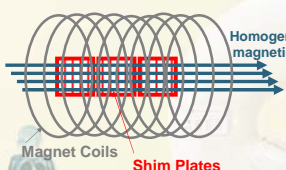
### Magnetic – Shim System

- The Main Magnet ( $B_0$ )
- The Shim Magnet
  - Maintain homogeneity
    - Units of PPM
    - Parts per million
  - Passive or active
    - Passive (shim plates, no current)
    - Active (shim coils, requires current)
- The Gradient Magnet
- The RF Magnet ( $B_1$ )

*Image courtesy of Philips Medical*

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### Passive Shim



Homogeneous magnetic field

Magnet Coils

Shim Plates

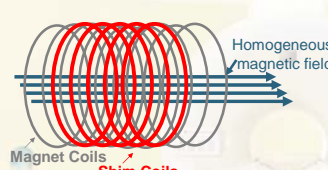
Shim plates

Magnet Enclosure

- Passive shim = NO current
- Shim plates within the imager near the magnet
- Shim plates are installed during imager manufacturing

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### Active Shim



Homogeneous magnetic field

Magnet Coils

Shim Coils


Shim

Magnet Enclosure

- Active shim implies current
- Shim coils within the imager near the magnet
- Shim coils are resistive magnets and require current in order to run
- Systems typically shimmed by the service engineer

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### Homogeneity



- Homogeneity is expressed in units of ppm
- PPM = parts per million or one 1/1,000,000
- 1T = 10,000 g
- 1 ppm inhomogeneity = + or - .01 gauss
- Field strength can be 10,000.01 g to 10,000.00 g
- if the frequency is 42 megahertz (million hertz)
- then the homogeneity is 42 Hz

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### Shim Power Supply

- Located within the equipment room
- Must be “on” for the shim system to work
- Otherwise homogeneity suffers
- Image quality is compromised

*Image courtesy of Philips Medical*

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### Gradient “Magnetic” System

- The Main Magnet ( $B_0$ )
- The Shim Magnet
- The Gradient Magnet
  - Spatial localization
  - Refocus Signals
  - Linear gradation (slope)
  - Time varied magnetic field
  - Units
    - Millitesla per meter (Mt/m)
    - Gauss per centimeter (g/cm)
    - 10 Mt/m = 1 g/cm
- The RF Magnet ( $B_1$ )

*Image courtesy of Philips Medical*

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### Gradient Configurations

X gradient  
Right to Left

Y gradient  
Anterior to Posterior

Z gradient  
Superior to inferior

**Isocenter**  
Center of three gradients

Gradient assembly

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### Wire Configurations for Gradient Coils

The main magnet adds to the gradient magnet to make this end higher

Direction of the current in the magnet coils

Direction of the current in the gradient

$B_0$

Magnet Coils

The gradient magnet subtracts from the main magnet to make this end lower

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### Dual Gradients

Typical gradient

Stronger gradient  
Typically for Neuro or Cardiac

Static field  $B_0$

Z gradient  
Superior to inferior

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### Gradient Shim

Gradient compensation

Static field  $B_0$

Inhomogeneity  
In Static field  $B_0$

Z gradient  
Superior to inferior

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### Gradient Units

**Gradients can be expressed in several units of measure including:**

- Strength (amplitude)
  - mT/M (millitesla per meter)
- Strength (amplitude)
  - g/cm (gauss per centimeter)
- 10 mT/M = 1 g/cm
- Rise Time  $\mu$  (microseconds)
  - (time to reach maximum amplitude)
- Slew Rate (combines rise time with strength)
  - Tesla per meter per second (T/M/s)
- Duty cycle (% of time the gradient can "work")

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### Gradient Amplifiers

- X, Y, Z gradient amps
- Each has master/slave configuration
- Located in the computer room
- Uses resistive components
- Requires current

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### Electromagnetic Radio Wave

- The Main Magnet ( $B_0$ )
- The Shim Magnet
- The Gradient Magnet
- The RF Magnet ( $B_1$ )
  - To excite the proton spins
  - $B_1$  field
  - Oscillating magnetic field
  - Larmor Frequency





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### Resonance

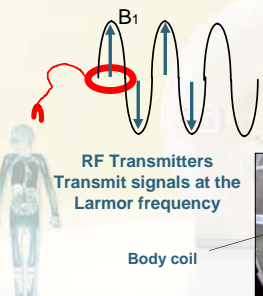
- RF coils
  - Transmitters
  - Receivers
- Body coil
- Local coils
  - Linear
  - Quadrature
  - Phase array
  - Coil elements



Images courtesy of Philips Medical


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### RF Transmitter Configurations



RF Transmitters Transmit signals at the Larmor frequency

Body coil




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### Transmit Coil Configurations

#### Vertical Field

Transmit coils on the "face" of the magnet poles



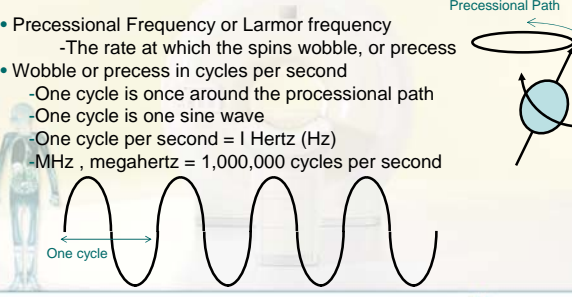
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### The RF Frequency

#### The Larmor Equation

-calculates the precessional frequency based on  $B_0$

- Precessional Frequency or Larmor frequency
  - The rate at which the spins wobble, or precess
- Wobble or precess in cycles per second
  - One cycle is once around the precessional path
  - One cycle is one sine wave
  - One cycle per second = 1 Hertz (Hz)
  - MHz, megahertz = 1,000,000 cycles per second



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### Larmor Frequency

In order to calculate the precessional (Larmor) frequency

- The magnetic moment of the proton
- The spin angular momentum of the proton

Gyro-magnetic ratio =  $\gamma$   
 Magneto-gyric ratio =  $\gamma$

•The field strength of the magnet

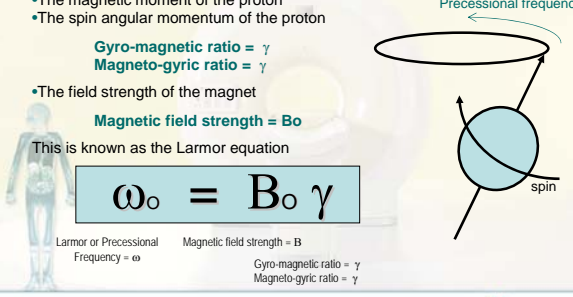
Magnetic field strength =  $B_0$

This is known as the Larmor equation

$$\omega_0 = B_0 \gamma$$

Larmor or Precessional Frequency =  $\omega$       Magnetic field strength =  $B$

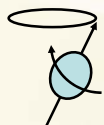
Gyro-magnetic ratio =  $\gamma$   
 Magneto-gyric ratio =  $\gamma$



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## Calculating the Larmor Frequency



$$\omega_0 = B_0 \gamma$$

$\omega$  for 1H (hydrogen) = 42.6 MHz/T  
If the Field strength ( $B_0$ ) is 1.0 Tesla

$\omega$  for 1H (hydrogen) = 42.6 MHz/T  
If the Field strength ( $B_0$ ) is 1.5 Tesla

Then...

$$\omega_0 = (1.0T) \times (42.6 \text{ MHz/T})$$

$$\omega_0 = 42.6 \text{ MHz (Megahertz)}$$

Then...

$$\omega_0 = (1.5T) \times (42.6 \text{ MHz/T})$$

$$\omega_0 = 63.9 \text{ MHz (Megahertz)}$$

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## Radiofrequency Energy?

### • Do we use radiation in MR?

### • Electromagnetic spectrum

### • X-rays

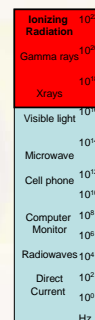
– High energy

– Ionizing radiation

### • MR Radiofrequency

– Low energy

– Non-ionizing



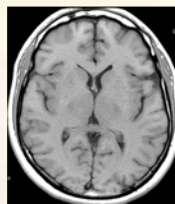
At 1.5T the frequency is roughly 64 MHz.  
In most cities, channel 3 broadcasts at roughly 64 MHz.

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## Head Coil



Images courtesy Philips

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## RF Coils



MAGNETOM Concerto



Body Spine Array Coil is available in S, M, L, XL. The Coil Kit includes size M and L.

### Special coil kit



CP Head/Neck Array Coil  
2 channel array receive coil  
2 additional neck coil elements

Extremity Array Coil, small and large.  
Dual phased array receive coils with 2 coil elements each

Internal dimensions (WxHxD):  
Small coil: 6 x 6.3 x 8.3 in  
Large coil: 7.8 x 8.3 x 8.3 in

Multipurpose Coil 4.3 in  
Single channel receive coil

Shoulder Array Coil  
Dual Phased Array receive coil  
Inner vertical opening 7.6 in

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## Building Coils



Coil tuning



Oscilloscope

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## RF Amplifiers

- Generates RF
- Amplifies signals
- Uses resistive components
- Requires power




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### RF Shielding

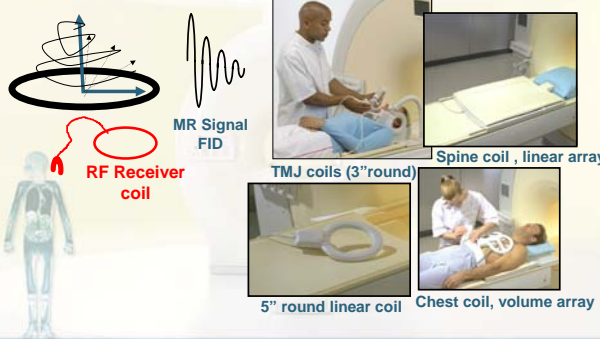


Use of copper to construct a Faraday Cage around the system  
Eliminate RF noise from the environment

Image courtesy Lindgren

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### RF Receiver Configurations



MR Signal FID

RF Receiver coil

5" round linear coil

TMJ coils (3" round)

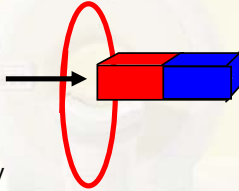
Spine coil, linear array

Chest coil, volume array

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### Faraday's Law of Induction

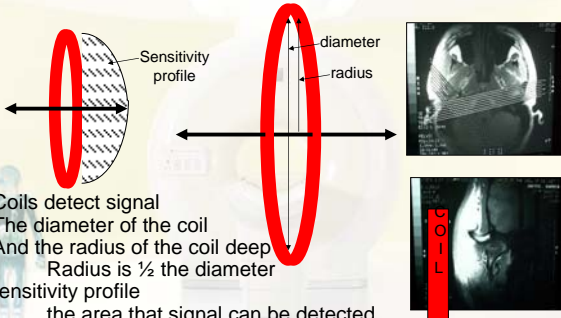
- Drag a magnet across a conductor, a voltage is created (induced) within the conductor



- $\frac{dB}{dt} = \frac{dV}{dt}$   
Change of magnet divided by time = voltage
- $\Delta B / \Delta t = \Delta V$

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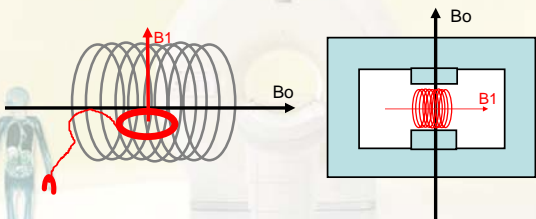
### Sensitivity Profiles for Coils



- Coils detect signal
- The diameter of the coil
- And the radius of the coil deep
- Radius is  $\frac{1}{2}$  the diameter
- Sensitivity profile the area that signal can be detected

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### Magnet / Coil Configurations

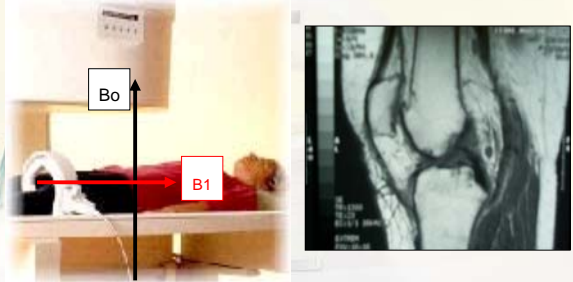


Bo

B1

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### Coil Orientation for vertical Bo



Bo

B1

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### Coil Orientation for horizontal Bo

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### Linear Coil

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### Helmholtz Pair

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### Induced signals in MR

**Linear coils** are like antennas...  
Electrons in the antenna are forced up-  
when the signal is heading up, and  
down, when down

**Quadrature coils** are like antennas...  
configured perpendicularly  
Signal is forced up, down and to the  
side, thus better signal!

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### Quadrature Coil

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### Phased Array

4 Coil Linear Array

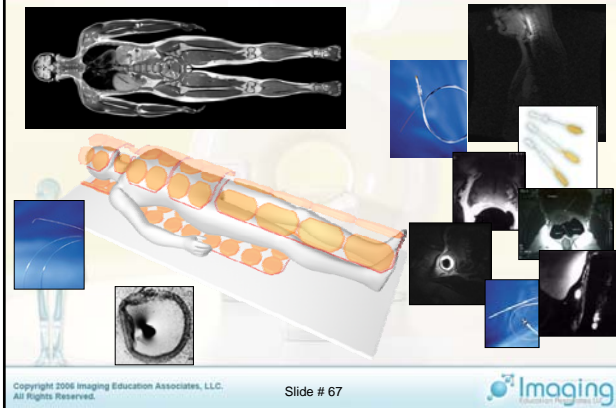
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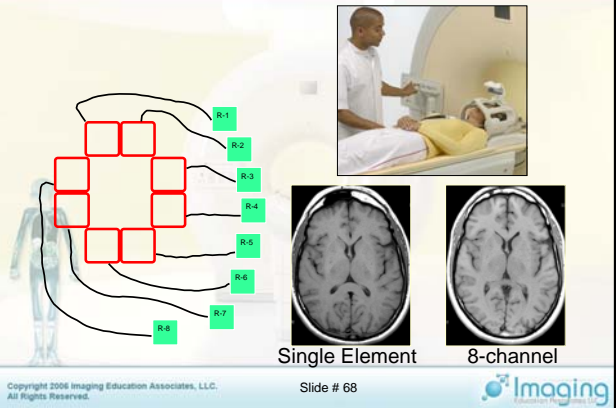
Imaging



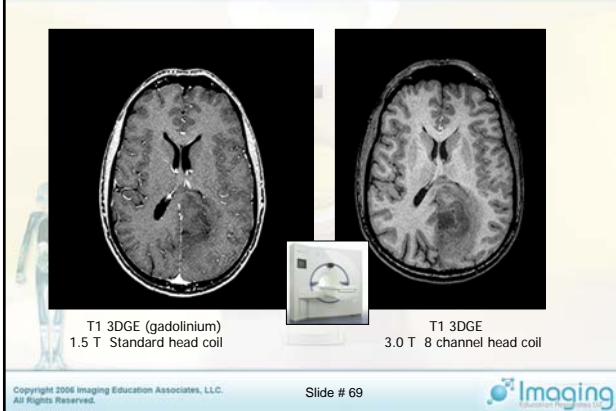
## Coils, Coils, Coils



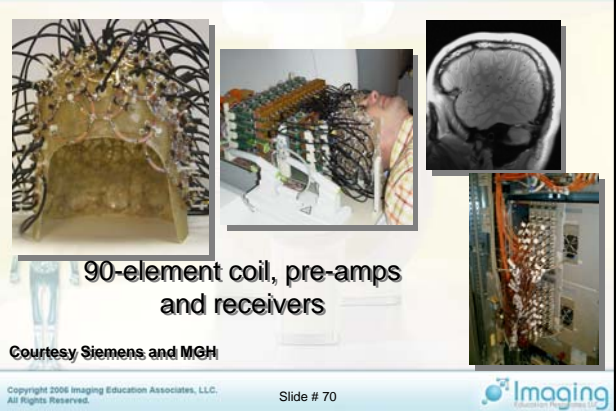
## 8 Channel Array



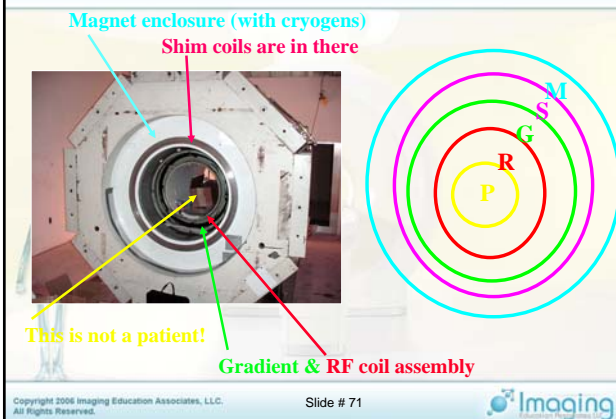
## Image Quality for field strength and Coils



## On the Horizon?



## All the coils in the MR imager



## 2.1 Instrumentation

Magnetism & MR Magnets  
other MR system components: shim systems,  
RF system, gradient system, other components

Thank you for your attention!

Click to take your post test and get your credits

Carolyn Kaut Roth, RT (R)(MR)(CT)(M)(CV) FSMRT  
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